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RESEARCH ARTICLE



## Facial muscle reanimation by transcutaneous electrical stimulation for peripheral facial nerve palsy

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### ABSTRACT

Reanimation of paralysed facial muscles by electrical stimulation has been studied extensively in animal models, but human studies in this field are largely lacking. Twenty-four subjects with a peripheral facial nerve palsy with a median duration of three years were enrolled. We studied activations of four facial muscles with electrical stimulation using surface electrodes. In subjects whose voluntary movement was severely impaired or completely absent, the electrical stimulation produced a movement that was greater in amplitude compared with the voluntary effort in 10 out of 18 subjects in the *frontalis* muscle, in 5 out of 14 subjects in the *zygomaticus major* muscle, and in 3 out of 8 subjects in the *orbicularis oris* muscle. The electrical stimulation produced a stronger blink in 8 subjects out of 22 compared with their spontaneous blinks. The stimulation could produce a better movement even in cases where the muscles were clinically completely paretic, sometimes also in palsies that were several years old, provided that the muscle was not totally denervated. Restoring the function of paralysed facial muscles by electrical stimulation has potential as a therapeutic option in cases where the muscle is clinically paretic but has reinnervation.

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Facial paralysis; functional electrical stimulation; prosthetics; rehabilitation

## Introduction

Facial nerve palsy is a condition that has important medical and social consequences for the affected individual. Deficit in blinking and eye-closure is the most important medical concern as it predisposes the cornea to drying and abrasion. Weakness in facial muscles is also associated with oral incompetence that causes drooling and difficulties in eating and drinking. The loss of symmetric facial expression complicates the communication of emotions and can affect quality of life [1]. The most common form of facial nerve palsy is Bell's palsy, with an incidence of around 25 out of 100,000 individuals per year [2], and accounts for more than a half of all facial nerve palsies [3]. The outcome of Bell's palsy is usually good. However, 10% to 30% of patients are left with residual weakness, asymmetry, or otherwise impaired function [2–4]. Other aetiologies such as traumas, tumours or infections have variable and often less favourable prognoses.

Current options for the restoration of facial symmetry and function comprise physical therapy, botulinum toxin injections, and surgical interventions. Although various types of physical therapies have been proposed, the evidence on their benefits is somewhat contradictory [5,6]. Botulinum toxin injections can be used to alleviate synkinesias and spasms and to improve symmetry by weakening the healthy side [7]. Surgical interventions aim to assist eye-closure, to improve rest symmetry, or to restore the movements of the paralysed side of the face. The interventions aiming to restore the dynamic function of the paralysed face include cross-facial nerve grafts [8], masseter to facial nerve transfers [9], and temporalis muscle [10] and free microvascular muscle transfers [11]. While these interventions can be very helpful in the restoration of facial symmetry and function, these techniques are demanding and not suitable for all patients. Thus, other treatment options to reanimate the paralysed face are needed.

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The principle of the reanimation of paralysed facial and laryngeal muscles with electrical stimulation has been studied since the 1970's in several experimental models. During these experiments, investigators measured the activity of the intact muscles of the contralateral side and, using this information, stimulated the paralysed side. The technique is referred to in the literature as electronic pacing. Electronic pacing has been studied for the activation of denervated or reinnervated facial and laryngeal muscles in different animal models [12–15]. In a rabbit model, electrical stimulation with implanted electrodes has been shown to be feasible even over the longer term, i.e., months [16]. More recently, electronic pacing has been studied in an experimental nerve lesion to produce an eye blink in rabbits [17] and in the facial muscles of rats [18,19]. Despite several animal studies, studies on humans have so far been scarce. Eliciting an eye blink with electrical stimulation has been studied to some extent [20,21]. Moreover, the principle of facial pacing on humans has been demonstrated on the *frontalis* muscle that was temporarily paralysed with local anaesthetics [22]. However, human studies on the reanimation of paralysed facial muscles other than *orbicularis oculi* are currently largely lacking.

In the present study, our goal was to study the feasibility of electrical stimulation with surface electrodes for the reanimation of different facial muscles in subjects with a peripheral facial nerve palsy. The *frontalis*, *zygomaticus major*, *orbicularis oris*, and *orbicularis oculi* muscles were stimulated in an attempt to produce forehead wrinkle, smile, lip pucker, and eye blink, respectively.

## Methods

### Subjects

Twenty-four patients (10 men, 14 women), aged 23 to 71 years ( $M = 51$ ,  $SD = 13$ ), presenting with a peripheral facial nerve palsy were recruited to the study after a patient database search or during outpatient visits to the Department of Otorhinolaryngology, Tampere University Hospital, Finland ( $n = 14$ , subjects 1 to 14, or Tampere group) and the Department of Plastic Surgery, Helsinki University Hospital, Finland ( $n = 10$ , subjects 15 to 24, or Helsinki group). The duration of the palsy ranged from 4 months to 59 years ( $M = 10$ , Median = 3 years). The most common single cause of the paresis was Bell's palsy (10 subjects), followed by a vestibular nerve schwannoma (four subjects) (Table 1).

The study was approved by the Ethics Committee of Pirkanmaa Hospital District. The participants volunteered and signed a written consent form concerning the participation and a separate consent form for the use of the video and photographic material.

### Assessment of the palsy

The severity of the palsy was individually assessed with the Sunnybrook facial grading system (SFGS) [23] that was scored offline by three investigators from a video recording, and with a nerve conduction study (NCS) and needle electromyography (EMG). SFGS is a composite score that evaluates the rest symmetry, symmetry of the movements, and synkinesias, ranging from zero (total paralysis) to one hundred (normal facial function). The SFGS score ranged from 11 to 78 ( $M = 37$ ,  $SD = 19$ ).

The NCS and needle EMG data were obtained from 21 subjects. Three subjects declined the examination. Numeric data for the bilateral NCS of the facial nerve were available from 16 subjects. The compound muscle action potential amplitude registered from the nasalis muscle ranged between 0.0 and 1.8 mV ( $M = 0.8$ ,  $SD = 0.6$ ) for the paralysed side and from 0.9 to 2.3 mV ( $M = 1.7$ ,  $SD = 0.5$ ) for the unaffected side. Needle EMG data were available for the *frontalis* and *orbicularis oris* muscles from all 21 subjects and for the *orbicularis oculi* muscle from 20 subjects. Five subjects had signs of ongoing reinnervation in at least one muscle. Four subjects had a finding of total denervation of at least one muscle. The severity of the neurogenic damage in the needle EMG data correlated positively to the degree of the paresis assessed with SFGS in the *frontalis* muscle ( $r_s = 0.701$ ,  $p < .001$ ). The correlation was not, however, significant between the needle EMG finding and the degree of the paresis in the *orbicularis oris* muscle ( $r_s = -0.307$ ,  $p > .05$ ) nor in the *orbicularis oculi* muscle ( $r_s = -0.063$ ,  $p > .05$ ).

### Equipment

The stimulator used in the experiment was developed and manufactured at the Faculty of Biomedical Sciences and Engineering, Tampere University of Technology [24]. The safety of the stimulation hardware complies with the standard IEC 60601–2–10 “Particular requirements for the basic safety and essential performance of nerve and muscle stimulators”. Our device's maximal current amplitude was limited to 48 mA, and the voltage amplitude was limited to 100 V. The pulse duration is controlled so that

**Table 1.** Background information of the subjects.

Subject number	Age	Duration of the palsy (years)	SFGS score	Aetiology	Surgical procedures
1	43	3	28	Suspected Lyme disease	
2	54	0.4	78	Bell	
3	60	3	61	Bell	Eyelid operation
4	29	2	54	Bell	
5	51	21	34	Bell	
6	55	1	70	Bell	Punctoplasty
7	48	3	18	Ramsay-Hunt syndrome	
8	48	0.3	37	Bell	
9	57	0.3	31	Ramsay-Hunt syndrome	
10	23	4	31	Bell	
11	58	3	74	Parotid tumour extirpation	
12	39	7	34	Bell	
13	50	48	27	Neck abscess	Unspecified nerve grafting, midface lift
14	44	3	49	Ear canal operation	
15	46	1	34	Vestibular nerve schwannoma	
16	71	1	11	Parotid tumour extirpation	Masseter to facial nerve transfer, nerve graft from facial nerve stump to zygomatic branches, microvascular subcutaneous flap from thigh
17	41	8	34	Bell	Gold weight
18	67	59	24	Unspecified ear operation	Fascial slings, gold weight
19	68	0.5	18	Parotid tumour extirpation	Masseter to facial nerve transfer, nerve graft from facial nerve stump to buccal branches, gold weight, fascial slings
20	68	45	49	Bell	Brow lift, lateral tarsal strip, midface lift, fascial slings, entropion operation
21	63	8	32	Vestibular nerve schwannoma	Fascial slings, platinum weight
22	42	2	21	Vestibular nerve schwannoma	Gold weight, cross facial nerve graft, masseter to facial nerve transfer
23	32	2	25	Vestibular nerve schwannoma	Platinum weight, cross facial nerve graft, masseter to facial nerve transfer
24	69	17	17	Multiple meningiomas	Gold weight, brow lift, facelift, fascial slings

the energy of the single pulse does not exceed what is set in the standard. The stimulation parameters that produced the best facial muscle activations in healthy individuals in a preliminary pilot testing were chosen for the experiment. A one-second-long train of bipolar rectangular pulses with a phase duration of 0.4 ms and a frequency of 250 Hz were used for the stimulation of the *frontalis*, *zygomaticus major*, and *orbicularis oris* muscles. The same stimulation parameters were used for the stimulation of the *orbicularis oculi* muscle except for the length of the stimulation train, which was set at 0.08 s in order to elicit an activation mimicking the duration of a natural eye-blink [25]. Five

trains of stimuli were delivered with an approximately one-second inter-train interval. Commercial adhesive pre-gelled electrodes (Quirumed<sup>®</sup>, GMDASZ Manufacturing Co., Ltd., Shenzhen, China) were used for the stimulation. The surface area of the electrodes was manually trimmed to approximately 1.5 cm<sup>2</sup>. The skin was prepared with an alcohol swab before the adhesion of the electrodes.

### Procedure

The *frontalis*, *orbicularis oculi*, *zygomaticus major*, and *orbicularis oris* muscles were stimulated one at a time.

The stimulation sites were chosen according to previously described guidelines for EMG measurements [26]. The stimulation was started at the current amplitude level of 0.5 mA and the current amplitude was raised at 0.5 mA steps. For the *frontalis*, *zygomaticus major*, and *orbicularis oris* muscles, the stimulation was continued until the subject asked to stop or when an amplitude limit of 10 mA was reached (patients 1 to 14 from the Department of Otorhinolaryngology, Tampere University Hospital, Tampere group). For subjects 15 to 24 from the Department of Plastic Surgery, Helsinki, Finland (Helsinki group) who had a more severe palsy, had undergone more surgical interventions, and were expected to have a higher excitation threshold, there was no preset upper limit for the stimulation current. Instead, the stimulation was continued until the subject asked to stop. The stimulation was also stopped if the safety settings of the device prevented the stimulation from continuing. In the case of the *orbicularis oculi* muscle, the stimulation was continued until a complete eye-closure was observed by two investigators during the online analysis, or until the subject asked to stop.

After the movement threshold was reached (i.e., some movement was observed by two investigators in the area of the stimulation during the online analysis), the subject was asked to give a pain rating on a scale of 1 to 9 (grade 1 meaning no pain and grade 9 meaning severe pain) after each set of five stimulus trains.

The order of the stimulation sites was counterbalanced so that the first stimulated muscle was either the *frontalis* muscle followed by the *orbicularis oculi*, *zygomaticus major*, and *orbicularis oris* muscles, the *zygomaticus major* muscle followed by the *orbicularis oris*, *frontalis*, and *orbicularis oculi* muscles, or the *orbicularis oris* followed by the *frontalis*, *orbicularis oculi*, and *zygomaticus major* muscles.

The stimulations were recorded with a Panasonic V750 digital video camera with 50 frames per second.

### Analysis

Two investigators independently performed an offline visual analysis of the video recordings in order to evaluate the electric current amplitude level at which a movement of the target muscle was produced (movement threshold), and the current amplitude level at which the maximal movement was achieved. In case of a discrepancy between the two estimations, the videos were reanalysed together by the two investigators to reach a consensus. Possible activations of

other muscles alongside the target muscle were also noted. The effect of the stimulation was evaluated and compared with the maximal voluntary activations of the corresponding function of the *frontalis*, *zygomaticus major*, and *orbicularis oris* muscles. In the case of eye blink, the stimulated blink was compared with the most complete spontaneous eye blink of the paralysed side. Two subjects were excluded of the analyses concerning the *orbicularis oris* muscle because of a poor electrode contact due to a beard. Another two subjects were excluded from the analyses concerning the *orbicularis oculi* muscle, one due to video recording failure and the other due to squeezing of the eyes during the stimulation, making the visual analysis of the stimulation-induced blinks impossible.

A cross-tabulation analysis and a Chi-square test of independence were used to evaluate the relationship between the needle EMG findings and the stimulated activations in the *frontalis*, *orbicularis oris*, and *orbicularis oculi* muscles. The needle EMG findings were categorised into five classes: complete denervation, severe denervation, moderate denervation, slight denervation, and normal. The stimulated activations were categorised into two classes: no movement and some movement. A Mann–Whitney test was used to compare the differences in the movement threshold for the different muscles between the Tampere and Helsinki groups.

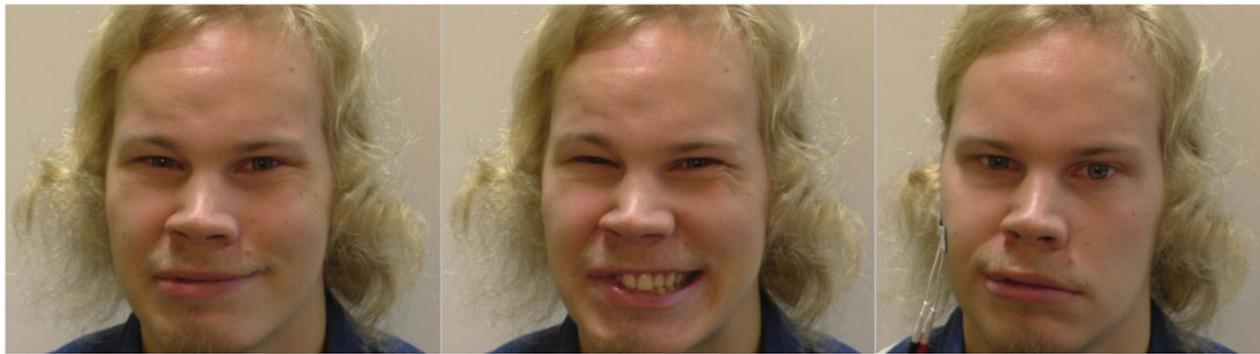
### Results

Results of the stimulations by subject are presented in [Supplements 1, 2, 3, and 4](#). Those subjects who had the most severe paresis of the *frontalis*, *zygomaticus major*, and *orbicularis oris* muscles (SFGS subscore 1 or 2 for the corresponding function) and whose eye blink was defective are discussed in more detail below. The stimulation produced a better (larger in amplitude) movement in 6 out of the 12 subjects with no voluntary movement (SFGS subscore 1) and in 4 out of the 6 subjects with a minor voluntary movement (SFGS subscore 2) of the *frontalis* muscle ([Supplement 1](#)). Examples of the stimulated movements compared with the voluntary movement are presented in [Figure 1](#) and [Supplementary Video 1](#).

The electrical stimulation produced a better movement in 3 out of the 7 subjects with no voluntary movement and in 2 out of the 7 subjects with a minor voluntary movement of the *zygomaticus major* muscle ([Supplement 2](#)). Examples of the stimulated movements compared with the voluntary movement are presented in [Figure 2](#) and [Supplementary Video 2](#).



**Figure 1.** Voluntary activation of the frontalis muscle (subject 13) compared with the stimulated activation at a current amplitude of 3.5 mA. The stimulated activation was considered better than voluntary activation.



**Figure 2.** Voluntary activation of the zygomaticus major muscle (closed-mouth and open-mouth smile, subject 10) compared with the stimulated activation at a current amplitude of 9.0 mA. The stimulated activation was considered slightly better than voluntary activation.

The electrical stimulation produced a better movement in 1 out of the 2 subjects with no voluntary movement and in 2 out of 6 subjects with a minor voluntary movement of the *orbicularis oris* muscle (Supplement 3). Examples of the stimulated movements compared with the voluntary movement are presented in Figure 3 and Supplementary Video 3.

The spontaneous blink on the paralysed side was defective in varying degrees in all but one subject. The stimulation produced a better blink in 4 out of 13 subjects whose spontaneous blink covered a maximum of half of the pupil and in 4 out of 9 subjects whose spontaneous blink covered more than half of the pupil (Supplement 4). In all cases where a movement could be produced, the subject's spontaneous or reflex blink was involved in, and thus facilitated the movement. An example of a spontaneous blink compared with a stimulated blink is presented in Figure 4 and Supplementary Video 4.

The movement thresholds (Table 2), defined as the lowest electric current amplitude that produced a

visible activation of the target muscle as evaluated in the offline video analysis, were significantly higher for the subjects from the Helsinki group compared with the subjects from the Tampere group.

Depending on the stimulated muscle, the stimulation spread in varying degrees to other muscles, most commonly to adjacent muscles. The spreading of the stimulation was the most evident during the stimulation of the *zygomaticus major* muscle. The muscles typically activated at the same time were the *zygomaticus minor*, *levator anguli oris*, and *orbicularis oculi* muscles. In two subjects with no visible or only a minor voluntary movement of the *zygomaticus major* muscle, however, the stimulation did not spread significantly to other muscles, producing a rather natural movement (Supplementary Video 2). Also, during the stimulation of the *frontalis* and *orbicularis oris* muscles, the stimulation often activated other muscles; typically, the *orbicularis oculi* muscle was activated during the stimulation of the *frontalis* muscle, and the *mentalis* and *depressor labii inferioris* muscles were activated



**Figure 3.** Voluntary activation of the orbicularis oris muscle (subject 22) compared with stimulated activation at a current amplitude of 19 mA. The stimulated activation was considered slightly better than voluntary activation.



**Figure 4.** A spontaneous blink compared with a stimulated blink (subject 14) at a current amplitude of 6.5 mA. The stimulated blink was considered better than the spontaneous blink.

during the stimulation of the *orbicularis oris* muscle, and sometimes more distant muscles.

The cross-tabulation results between the needle EMG finding and the stimulated activation in the *frontalis* muscle are shown in Table 3. A Chi-square test of independence was performed to study the relationship between the EMG finding and the stimulated activation in the *frontalis* muscle. The relationship between these was significant ( $\chi^2$  (4, 21) = 13.65,  $p < .01$ ). In cases of complete denervation, the stimulation did not produce any visible movement, whereas when the degree of denervation was moderate, slight,

or the EMG finding was normal, the stimulation produced a movement.

The cross-tabulation results between the needle EMG finding and the stimulated activation in the *orbicularis oris* muscle are shown in Table 4. The Chi-square test showed that the relationship between the needle EMG finding and the stimulated activation in the *orbicularis oris* muscle was significant ( $\chi^2$  (3, 21) = 11.966,  $p < 0.01$ ). Again, if the denervation was total, the stimulation did not elicit any visible movement. In cases where the denervation was severe, and in most of the cases the denervation was moderate,

**Table 2.** Mean electric current amplitudes at the movement threshold.

Stimulated muscle	Mean amplitude (mA) ± SD to movement		Mann–Whitney test
	Tampere group	Helsinki group	
<i>Frontalis</i>	2.4 ± 0.5 (n = 13)	5.2 ± 2.2 (n = 5)	U = 2.0, p < 0.01
<i>Zygomaticus major</i>	5.6 ± 1.6 (n = 11)	9.9 ± 1.9 (n = 4)	U = 0.0, p < 0.01
<i>Orbicularis oris</i>	3.1 ± 1.0 (n = 12)	6.8 ± 3.0 (n = 6)	U = 6.0, p < 0.05
<i>Orbicularis oculi</i>	2.3 ± 0.9 (n = 12)	4.7 ± 2.2 (n = 5)	U = 9.5, p < 0.05

**Table 3.** Cross-tabulation results between the needle EMG finding and the stimulated activation in the *frontalis* muscle.

	Stimulation result for <i>frontalis</i> muscle		
	No movement	Movement	Total
Needle EMG finding			
Complete denervation	3	0	3
Severe denervation	2	4	6
Moderate denervation	0	9	9
Slight denervation	0	2	2
Normal	0	1	1
Total	5	16	21

the stimulation elicited visible movement, whereas in three of the four cases where the denervation was slight, no visible movement occurred.

The cross-tabulation results between the needle EMG finding and the stimulated activation in the *orbicularis oculi* muscle are shown in Table 5. The chi-square test showed no significant relationship between the needle EMG finding and the stimulated activation in the *orbicularis oculi* muscle ( $\chi^2$  (4, 18) = 4.661,  $p > 0.05$ ). However, the frequencies in Table 5 suggest that the stimulation was more likely to be successful in those cases where the degree of denervation was slight.

In subjects for whom the stimulation produced at least some movement, the mean pain rating at the level of the maximal movement was 5.5 (SD ± 2.5, range 1 to 9) for the *frontalis* muscle, 5.8 (SD ± 2.9, range 1 to 9) for the *zygomaticus major* muscle, 5.3 (SD ± 2.6, range 2 to 9) for the *orbicularis oris* muscle, and 4.3 (SD ± 2.6, range 1 to 9) for the *orbicularis oculi* muscle. In the case of the *orbicularis oculi* muscle, the two abovementioned subjects and one subject whose stimulus-induced blink could not be distinguished from the reflex blinking, resulting in no pain rating, were not included.

## Discussion

A considerable number of individuals who are affected by a peripheral facial nerve palsy are left with residual symptoms that have consequences in their everyday life. Several of our subjects had undergone more or less extensive surgical interventions to restore facial symmetry and function. While many of them had benefited from the surgery, they still had unresolved

**Table 4.** Cross-tabulation results between the needle EMG finding and the stimulated activation in the *orbicularis oris* muscle.

	Stimulation result for <i>orbicularis oris</i> muscle		
	No movement	Movement	Total
Needle EMG finding			
Complete denervation	1	0	1
Severe denervation	0	7	7
Moderate denervation	1	8	9
Slight denervation	1	1	2
Normal	0	0	0
Total	3	16	19

**Table 5.** Cross-tabulation results between the needle EMG finding and the stimulated activation in the *orbicularis oculi* muscle.

	Stimulation result for <i>orbicularis oculi</i> muscle		
	No movement	Movement	Total
Needle EMG finding			
Complete denervation	1	0	1
Severe denervation	1	3	4
Moderate denervation	2	7	9
Slight denervation	0	3	3
Normal	0	1	1
Total	4	14	18

issues, such as a defective eye blink and drooping forehead. The subjects who had not had operative treatments and had achieved a nearly normal resting symmetry through spontaneous recovery, still reported problems caused by the defective function of the facial muscles that were either medically or socially disabling, such as problems with eye health and the inability to smile.

To the best of our knowledge, our study is the first one that has investigated the restoration of the function of facial muscles other than *orbicularis oculi* by electrical stimulation in persons with a facial nerve palsy. Frigerio et al. [21] have recently reported that transcutaneous electrical stimulation produced a complete eye closure in 55% of participants with acute facial nerve palsy when the zygomatic facial nerve branch was stimulated. In the present study, we focussed on subjects who had passed the acute phase, many having a paresis with a duration of several years. In our study, the success rate in producing a stronger

stimulated blink compared with the individual's spontaneous blink was 36%. Regarding the other stimulated muscles, in cases where the function of the muscle was severely defective, the electrical stimulation produced a better movement than the voluntary activation in 56% of cases for the *frontalis* muscle, in 36% for the *zygomaticus major* muscle, and in 38% for the *orbicularis oris* muscle.

Our subjects presented palsies of variable durations and different causes, and therefore the generalisation of the results by aetiology is difficult since the number of subjects with a given cause was relatively small. We have shown, however, that activating facial muscles by electrical stimulation is possible in palsies with different causes and also in older palsies.

Except *frontalis* muscle, the clinical weakness of the muscle and the degree of the neurogenic damage seen in the needle EMG did not correlate significantly. As expected, the muscles showing a complete denervation in the needle EMG did not respond to electrical stimulation. Otherwise, the cross-tabulations showed that the level of neurogenic damage was in some extent, but not always, associated with successful stimulation. This conforms to our findings that a muscle may appear clinically paretic, but it can be activated by electrical stimulation if reinnervation exists.

The subjects in the Helsinki group required significantly higher stimulation currents in order to initiate a movement in the target muscle. Many of these subjects had a paralysis as a consequence of different neoplasias and supposedly more severe initial axonal damage, and hence poorer outcome than those with an idiopathic palsy. These subjects had also had more surgical interventions that cause scar formation, which may have affected the conductive characteristics of the tissues. The reported pain ratings at the electric current amplitude level that produced the maximal movement, as evaluated in the offline video analysis, varied from not painful at all to very painful, underlining the very high inter-individual variability for the acceptability of the electrical stimulation. In our previous study on healthy subjects [27], the participants often reported that even after giving a rather high pain rating, the stimulation was not actually painful but described it as otherwise uncomfortable. Whether this type of perceived discomfort would be acceptable in long-term use needs to be tested in future studies. It is, however, possible that the discomfort or pain caused by the stimulation may limit the method's usefulness at least in some individuals. All in all, reanimating facial muscles by electrical stimulation would not

be a one-size-fits-all kind of treatment, but rather a tailor-made solution with individually adjusted stimulation parameters and sites and number of electrodes.

Another limitation of our study is the visual analysis of the facial movements that is susceptible to subjective bias that we tried to minimise by using two evaluators. Currently, no method that could be considered as a gold standard to objectively analyse the stimulated facial movements exists, and we consider the analysis procedure we used was adequate for the objectives of our study.

Stimulation of the *zygomaticus major* muscle proved to be particularly challenging. The stimulation often spread to adjacent muscles, creating an unnatural appearance in respect to smiling. This finding is consistent with the results of our previous study on healthy subjects [27]. Spreading of the stimulation also occurred while stimulating other muscles; however, in these cases the activation of other muscles rarely produced expressions that would be considered disturbing or disfiguring. The difficulties in the electrical stimulation of the *zygomaticus major* muscle may result from spreading of the stimulus via facial nerve branches and from the greater distance between the electrode and the muscle due to adipose tissue. Whether experimenting with stimulation electrode locations as opposed to using predetermined locations would yield better results is worth further study.

The stimulator we used in this experiment had four stimulator channels, four channels for the EMG measurements, and freely adjustable stimulation waveform, thus providing flexible potential for future studies on facial pacing. In addition to defining appropriate stimulation parameters, facial pacing requires a reliable EMG or other muscle activation measurement method from the healthy side of the face [28]. The signal analysis and stimulation signal generation should be fast enough to produce a movement that is perceived as natural [29]. One of the possible future applications of electrical facial muscles is the development of a wearable/portable prosthesis that uses facial pacing technology. With this prospect, cosmetically acceptable electrodes should be developed.

In summary, the preliminary results presented in this study are promising regarding the reanimation of paralysed facial muscles with electrical stimulation. Traditionally, it has been believed that in a late recovered facial palsy the muscle function can no longer be regained after two or three years, and that a clinically spastic or non-functional muscle is scarred, shortened, or atrophied. Therefore, targeted reinnervation

attempts with nerve transpositions or nerve grafts are usually performed at one-year post palsy at the latest. Our study shows that muscles that have been clinically dormant for more than 10 years can function with targeted stimulation, if a subclinical innervation exists.

## Conclusions

Electrical stimulation has the potential for restoring the function of facial muscles even in facial nerve palsies that are several years old and where the muscle has no clinical functionality, provided the muscle is not completely denervated. Further studies are indicated to establish the efficacy, tolerability, and safety of the electrical stimulation, especially in a long-term use.

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## Availability of data and materials

Data and materials, with the exception of the videos, can be made available upon request to the authors.

## Disclosure statement

The authors declare that they have no competing interests.

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